Using Thoracic Ultrasonography to Accurately Assess Pneumothorax Progression During Positive Pressure Ventilation

A Comparison With CT Scanning

Nils Petter Oveland, MD; Hans Morten Lossius, MD, PhD; Kristian Wemmehund, cand med; Paal Johan Stokkeland, MD; Lars Knudsen, MD, PhD; and Erik Sloth, MD, PhD, DMsc

Background: Although thoracic ultrasonography accurately determines the size and extent of occult pneumothoraces (PTXs) in spontaneously breathing patients, there is uncertainty about patients receiving positive pressure ventilation. We compared the lung point (ie, the area where the collapsed lung still adheres to the inside of the chest wall) using the two modalities ultrasonography and CT scanning to determine whether ultrasonography can be used reliably to assess PTX progression in a positive-pressure-ventilated porcine model.

Methods: Air was introduced in incremental steps into five hemithoraces in three intubated porcine models. The lung point was identified on ultrasound imaging and referenced against the lateral limit of the intrapleural air space identified on the CT scans. The distance from the sternum to the lung point (S-LP) was measured on the CT scans and correlated to the insufflated air volume.

Results: The mean total difference between the 131 ultrasound and CT scan lung points was 6.8 mm (SD, 7.1 mm; range, 0.0-29.3 mm). A mixed-model regression analysis showed a linear relationship between the S-LP distances and the PTX volume (P < .001).

Conclusions: In an experimental porcine model, we found a linear relation between the PTX size and the lateral position of the lung point. The accuracy of thoracic ultrasonography for identifying the lung point (and, thus, the PTX extent) was comparable to that of CT imaging. These clinically relevant results suggest that ultrasonography may be safe and accurate in monitoring PTX progression during positive pressure ventilation.

CHEST 2013; 143(2):415–422

Abbreviations: CXR = chest radiograph; PTX = pneumothorax; S-LP = sternum-lung point

Physical examination, including lung auscultation, is insufficient for diagnosing a pneumothorax (PTX) in blunt trauma victims. The most common adjunct used to evaluate a PTX is the plain chest radiograph (CXR) but this modality has a low sensitivity for detecting intrapleural air in patients with trauma, who are typically confined in the supine position for spinal immobilization. As a consequence, more than...
Materials and Methods

This was a laboratory study of a PTX in a porcine model. Qualified and experienced animal caretaker personnel monitored the health of the animals during the study period. The experiments complied with the guidelines for animal experimental studies issued by the Danish Inspectorate for Animal Experimentation under the Danish Ministry of Justice, which also approved the study. The study adhered to the principles in the Guide for the Care and Use of Laboratory Animals.16

Animal Model

Three female Danish Landrace pigs (mean ± SD body weight = 56.0 ± 2.0 kg) were used (supplied from a local farm owned by Aarhus University). The animals were anesthetized with a combination of fentanyl, ketamine, and propofol; intubated; and positive pressure ventilated using a transport respirator (Oxylog 3000; Dräger) set to a tidal volume of 750 mL, a respiratory rate of 15 breaths/min, a positive end-expiratory pressure of 2 to 5 cm H2O, and an FIO2 of 30%. The end-tidal CO2 level was kept within the normal range (4.0-6.5 kPa). All the animals were monitored by ECG, and their core temperatures, invasive arterial BPs, oxygen saturations, and end-tidal CO2 levels were trended. In the radiology department, the animals were fixed in the supine position on a CT scan table. A three-way stopcock catheter (BD Connecta; Becton, Dickinson and Company) was inserted into the pleural space through a small thoracotomy at the intersection of the fifth to the seventh intercostal space and the anterior axillary line (Fig 1). The catheter was then anchored to the surrounding muscle and fascia. Bilateral (n = 2) and unilateral (n = 1) PTXs were induced by incrementally injecting and withdrawing air from the pleural cavity using a 50-mL syringe (Omnifix, 50 mL; B. Braun Medical Inc) connected to the catheter. At the conclusion of the data collection, the animals were killed with an injection of pentobarbital.

Diagnostic Tests

Diagnostic ultrasound and CT scan thoracic evaluations were performed at 10 different PTX volumes. The PTX volumes were: 50, 100, 150, 200, 300, 400, 500, 600, 500, and 200 mL.

Ultrasoundography: The ultrasound scans were performed by two experienced anesthesiologists using a Vivid Q ultrasound machine (General Electric Company) with a 12L-RS multifrequency 6-13 MHz linear array transducer (General Electric Company). To map the PTX topography, the ultrasound images were recorded on a CT scan table. A three-way stopcock catheter (BD Connecta; Becton, Dickinson and Company) was inserted into the pleural space through a small thoracotomy at the intersection of the fifth to the seventh intercostal space and the anterior axillary line (Fig 1). The catheter was then anchored to the surrounding muscle and fascia. Bilateral (n = 2) and unilateral (n = 1) PTXs were induced by incrementally injecting and withdrawing air from the pleural cavity using a 50-mL syringe (Omnifix, 50 mL; B. Braun Medical Inc) connected to the catheter. At the conclusion of the data collection, the animals were killed with an injection of pentobarbital.

CT Imaging: To define the extension of the intrapleural air collection, a non-contrast-enhanced CT scan was performed using a multislice CT scanner (Philips MX 8000 quad, Koninklijke Philips Electronics N.V.) with the following parameters: 120 kV, 120 to 150 mA, standard filter, 6.5-mm slice thickness, 3.2-mm slice increments, and a 310- to 360-mm field of view. A complete thoracic CT scan was obtained from the apex to the base during a short inspiratory hold period. The Digital Imaging and Communications in Medicine format pictures were stored and transferred to an archiving workstation. To optimize intrapleural air detection, the window width was adjusted to 1,500 Hounsfield units and the window level to −500 Hounsfield units.

Data Analysis

The accuracy of the ultrasound imaging for delineating the PTX extension was determined by measuring the distance from the pleural cavity using a 50-mL syringe (Omnifix, 50 mL; B. Braun Medical Inc) connected to the catheter. At the conclusion of the data collection, the animals were killed with an injection of pentobarbital.
Figure 2. Flowchart suggesting the correct sequence for ultrasound identification of the lung point. The lung point is localized at the interface between two distinct sonographic patterns that are synchronous with respiration: one with no lung sliding (the "stratosphere sign" in M-mode) and the other with normal lung sliding (the "seashore sign" in M-mode) illustrated in the lower right corner. Demonstration of normal lung sliding is only possible on video clips.
A total of 131 lung points were identified. The overall mean difference between the two modalities...
ultrasonography and CT imaging was 6.8 ± 7.1 mm, with colocation in the anterior, lateral, and posterior chest regions of 6.8 ± 6.6 mm, 6.4 ± 6.1 mm, and 7.3 ± 6.4 mm, respectively. The mean variance between the ultrasound and CT scan measurements of the lateral PTX limits was 0.0 to 29.3 mm (Table 1). Furthermore, there was a high level of agreement in the lung point measurements between readers one and two, as illustrated in the Bland-Altman plot (Fig 5). The 95% limits of agreement interval was −12.0 to 13.9.20

The mixed-model regression analysis revealed a linear relationship between the S-LP distance and the PTX volume  (P < .001). The strength of the relation between the S-LP distance and the PTX volume differed between the left and right lungs (P = .001), but this divergence decreased at larger PTX volumes (Fig 6). When the PTX volume increased by 100 mL, the mean S-LP distance increased by 4 mm (P < .001) in the right lung and by 11 mm in the left (P < .001) (95% CIs, 0.01–0.07 and 0.05–0.13, respectively). The effect of PTX volume on the S-LP distance did not vary with the chest level (P = .746), illustrated in Figure 6 by the parallel curves between the high and medium levels on both the right and left sides. With increasing PTX volumes, the lung point moved laterally and then medially with the subsequent withdrawal of air. Insufflation and deflation had the same absolute effect on the change in the S-LP distance (P = .904). The results of the mixed linear model analysis are summarized in Table 2.

**Discussion**

Our study demonstrates that there is a linear relationship between PTX volume and the lateral position of the lung point during mechanical ventilation, and that ultrasound imaging is as accurate as CT imaging for localizing lung points. These findings are clinically relevant and may enable physicians to use ultrasonography to accurately follow the progression of PTXs during positive pressure ventilation.

Although it may seem reasonable to consider the size of the PTX when making procedural decisions, a newly published large prospective observational study found PTX size not to be an independent predictor of observation failure (defined as the subsequent need for a chest drain) in patients with blunt trauma. The most striking findings were that the patients whose occult PTXs expanded were ≥70 times more likely to require chest tube drainage and that mechanical ventilation tripled this risk.21 This study used CXR imaging to assess the PTX progression, despite its being a poor method for detecting PTXs and one that underestimates the size.12,22 Two CT scan-based PTX classification systems, a linear size (thickness)-based algorithm23,24 and computer-aided volumetric measurements,25 have been suggested as potential guides for making treatment decisions, but no consensus on the clinical usefulness of these PTX scoring systems has been established.21

The conceptual basis for using bedside thoracic ultrasonography imaging in patients with occult PTX is that it is difficult to differentiate between medium- and large-sized PTXs, as evidenced by the weak correlation between increasing PTX volumes and the lateral position of the lung point on CT scans. They offered no statistical analysis or references to support this statement, only commenting on three CT images in the article. Soldati et al18 found a mean difference of 19 mm between ultrasound and CT scan lung points and they concluded that lung ultrasonography can be used to characterize PTX size and extension with an accuracy that approaches the reference standard. They excluded patients with occult PTX who needed mechanical ventilation because these patients often have more extensive and clinically significant PTXs. These assumptions may be invalid, because the occult PTX size and severity distributions in positive-pressure-ventilated patients are similar to nonintubated patients,5 and because clinically significant PTXs are equally frequent in both these patient groups.10

The remaining questions are whether an identifiable cohort of patients who are mechanically ventilated with occult PTX can be safely observed without undergoing tube thoracostomy,25 and how these patients should be monitored. The first question remains controversial, pending completion of prospective randomized trials, whereas the second is addressed in this experimental study. Our results (a mean difference between the ultrasound and CT scan locations of only 6.8 mm)
Unfortunately, the current study design, combined with the radiation hazard posed by serial CT scans, precludes using this experimental approach in human subjects. We do recognize some limitations. First, one pig had a small amount of pleural fluid in the basal part of the right hemithorax that could have affected the localization of the lung point. Second, the thoracotomies may have introduced small amounts of air into the pleural cavities when the catheters were introduced, thereby increasing the actual PTX volume beyond the insufflated air volumes specified in the study protocol. Although excessive air was withdrawn using a 10-mL syringe before starting the air injections, it is possible that some air remained in the pleural cavity. This residual air may explain the differences in the mean S-LP distances of the right and left hemithoraces with equal PTX volumes (Fig 6). Another explanation for this finding may be the anatomic asymmetry of the thorax, with the presence of the heart in the left hemithorax affecting the air distribution. Finally, a large PTX can eliminate the lung point sign completely because the lung totally collapses and loses contact with the interior wall of the chest cavity. These patients often experience respiratory distress due to diminished lung capacity.

demonstrate that ultrasonography is comparable to CT imaging for localizing the lung point during positive pressure ventilation in a porcine model. The linear response of the S-LP distance to the PTX volume implies that the lung point moves in a progressive arc from the anterior to the lateral and to the posterior aspect of the chest wall as the PTXs expand. This progression was assessed at two different chest levels and was independent of whether the PTX was increasing or decreasing in size (Fig 6, Table 2).

Porcine anatomy is not identical to human anatomy, but the respiratory and cardiovascular systems are similar; therefore, pigs are an important animal model in biomedical research. Before commencing this study, we validated our PTX model using the reference standard CT scan and found equal distribution of intrapleural air as in supine patients with trauma. This study also revealed that the PTX volume and lung point position could easily be altered through insufflation and deflation. We performed all our measurements at the CT scan laboratory, which reduced the risk of any PTX progression occurring between the ultrasound and the CT scans. Soldati et al allowed up to 1 h to elapse between their tests, whereas all our measurements were performed during an inspiratory hold and within minutes of each other.

Unfortunately, the current study design, combined with the radiation hazard posed by serial CT scans, precludes using this experimental approach in human subjects.

We do recognize some limitations. First, one pig had a small amount of pleural fluid in the basal part of the right hemithorax that could have affected the localization of the lung point. Second, the thoracotomies may have introduced small amounts of air into the pleural cavities when the catheters were introduced, thereby increasing the actual PTX volume beyond the insufflated air volumes specified in the study protocol. Although excessive air was withdrawn using a 10-mL syringe before starting the air injections, it is possible that some air remained in the pleural cavity. This residual air may explain the differences in the mean S-LP distances of the right and left hemithoraces with equal PTX volumes (Fig 6). Another explanation for this finding may be the anatomic asymmetry of the thorax, with the presence of the heart in the left hemithorax affecting the air distribution. Finally, a large PTX can eliminate the lung point sign completely because the lung totally collapses and loses contact with the interior wall of the chest cavity. These patients often experience respiratory distress due to diminished lung capacity.
A tension PTX is diagnosed clinically and requires immediate needle decompression without the diagnostic delay associated with CXR or ultrasound imaging. 

**CONCLUSIONS**

We have demonstrated that lung point movement is an indicator of PTX progression during positive pressure ventilation that can be evaluated as accurately by ultrasonography as by CT scanning. This finding may open up new possibilities for monitoring PTX development at the bedside. If a decision is made to observe patients who are mechanically ventilated with trauma and occult PTXs, we propose using serial thoracic ultrasound imaging to assess any PTX progression, which is known to be the strongest predictor of a patient’s need for chest tube insertion. Further research should focus on the relationship between the cutaneous projections of the lung point and the optimal treatment options.

**REFERENCES**


**Table 2—Mixed Linear Model Analysis of the Sternum to Lung Point Distance Relative to the Pneumothorax Volume on the Thoracic Insufflation Side and Chest Level**

<table>
<thead>
<tr>
<th>Variable</th>
<th>Coefficient</th>
<th>95% CI</th>
<th>P Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Intercept, mm</td>
<td>43.7</td>
<td>16.0 to 71.3</td>
<td>.010</td>
</tr>
<tr>
<td>Side&lt;sup&gt;+&lt;/sup&gt;</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>R</td>
<td>54.0</td>
<td>39.5 to 68.5</td>
<td>&lt;.001</td>
</tr>
<tr>
<td>L</td>
<td>0.0</td>
<td>Reference</td>
<td>...</td>
</tr>
<tr>
<td>Level&lt;sup&gt;+&lt;/sup&gt;</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>High</td>
<td>−20.6</td>
<td>−27.7 to −13.4</td>
<td>&lt;.001</td>
</tr>
<tr>
<td>Medium</td>
<td>0.0</td>
<td>Reference</td>
<td>...</td>
</tr>
<tr>
<td>Volume, mL</td>
<td>0.11</td>
<td>0.08 to 0.13</td>
<td>&lt;.001</td>
</tr>
<tr>
<td>Thoracic side (R) × volume</td>
<td>−0.067</td>
<td>−0.11 to −0.03</td>
<td>.001</td>
</tr>
<tr>
<td>Thoracic side (L) × volume</td>
<td>0.000</td>
<td>Reference</td>
<td>...</td>
</tr>
</tbody>
</table>

L = left; R = right.

<sup>+</sup>Right and left thoracic side; the left is the reference.

<sup>+</sup>Chest level; high is between costae 2 and 3; medium is between costae 5 and 6 (reference).


